#### ISMRM 2006 Educational Lecture

# Measuring Brain Volume Changes: The Tools

#### Measuring Brain Volume Changes: The Tools

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# • Tissue-type segmentation & bias field correction

- Longitudinal: temporal brain change
- Cross-sectional: single time point brain state
- Localised analyses



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## Segmentation example: FAST from FSL

• First use BET to remove non-brain





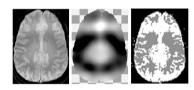
- Input can be single image (e.g. T1, T2, Proton Density)
- Or several of these ("multi-channel")
- For multi-channel, all must be aligned (e.g. with FLIRT)



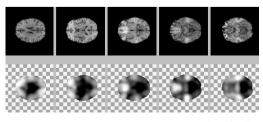




# MR Images - RF Inhomogeneity ("Bias Field")

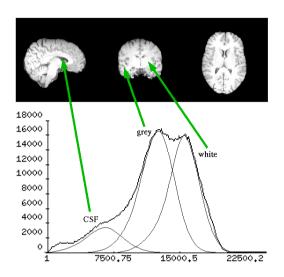


- RF Inhomogeneity causes intensity variations in image
- Causes problems for simple threshold-based segmentation
- Need to remove bias field before or within segmentation



# Histograms - Tissue Intensity Distributions

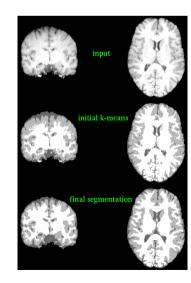
- Histogram = "voxel count vs intensity"
- Mixture of Gaussians
- Model class means and widths
- If well separated, clear peaks, i.e. segmentation easy
- But overlap worsened by: bias, blurring, low resolution, head motion



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# Using Spatial Neighbourhood Information (MRF)

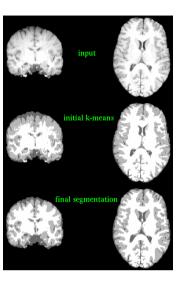
- Neighbourhood information: "if my neighbours are grey matter then I probably am too"
- Most methods (like the kmeans initialisation) don't use spatial neighbourhood information
- Reduces noise and increases robustness
- Carried out using MRF (Markov Random Field) model



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## **Initial Segmentation**

- Need to bootstrap method somehow initial segmentation
- Use "Tree-Structure K Means"
- Start with one class (Gaussian)
- Split & fit
- Re-split until enough classes
- Many other segmentations **only** do this step!



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#### At Last - the Overview!

- Initial segmentation tree-structure k-means
- Iterate
  - o Estimate bias field
  - Iterate segmentation
    - Update segmentation
    - Update tissue class parameters (mean and standard deviation)

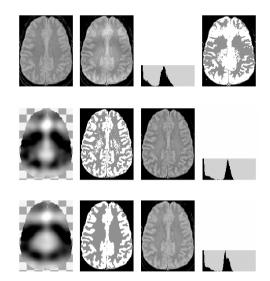


## **Examples - Single Channel Segmentation**

Original, original plus bias field, histogram, best thresholding segmentation

No MRF used: estimated bias, segmentation, restored image, histogram

With MRF



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## Longitudinal Change Analysis

Example: SIENA (Structural Image Evaluation, using Normalisation, of Atrophy, from FSL)

- Measures atrophy / general brain change
- Accurate and fully automatic
- Proven for a range of slice thicknesses
- Proven for a range of MRI sequences
- Accuracy 0.2% of brain volume
- Correction for scanner geometry drifts



## A-Priori Tissue Probability Maps

- A-priori maps created by averaging many aligned segmentations; can be used as priors in segmentation but can skew results
- If bias is very bad, priors can aid initial segmentation
- A-priori maps can also be optionally used to feed into final posteriors (e.g. to aid segmentation of deep gray); FAST doesn't use this by default, SPM2 does
- SPM5 improves the use of priors (compared with SPM2) by combining segmentation with alignment to priors.



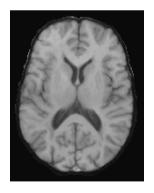


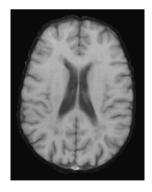




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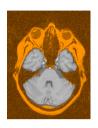
#### Example of Atrophy in Action





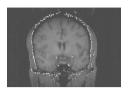
**BET**: Brain Extraction Tool

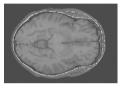
- Eliminates all non-brain tissue
- Accurate and fully automatic
- < 1 minute processing time

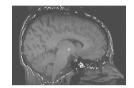


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- Estimation of exterior surface of skull
- Used to hold image scale constant in registration



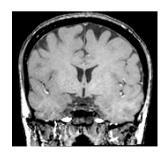




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## **FLIRT Linear Registration**

- Register brains (full affine)
- Apply to skulls then re-register skulls, altering only scale and skew (corrects for changes in scanner geometry etc.)
- Apply to brains then re-optimise rotation and translation
- Use transform's midway position
- < 10 minutes for 3-step registration



## Atrophy Measurement Using Edge Motion

Find brain/non-brain edge points in image 1 using FAST tissue segmentation (including bias-field correction)



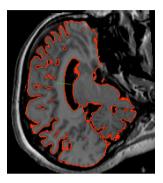


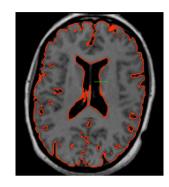




## Atrophy Measurement Using Edge Motion

## At each edge point take 1D perpendicular profile



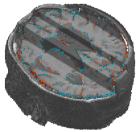


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## Atrophy Measurement Using Edge Motion

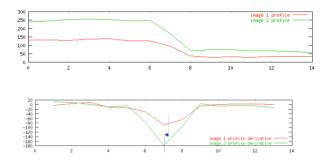
- Thus for each edge point in image 1 the perpendicular motion is found
- Insensitive to changes in imaging
- Mean motion over whole brain surface calculated
- Convert into % brain volume change (PBVC) by estimating brain surface area and volume and then doing selfcalibration





#### Atrophy Measurement Using Edge Motion

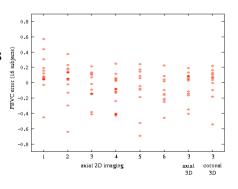
- Find profile from same point in image 2
- Take windowed derivative of both
- Correlate with subvoxel accuracy



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#### Error Plots from "Normals"

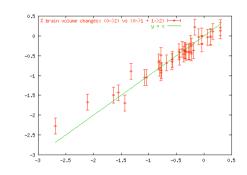
- 16 normals, each scanned twice
- Range of slice thicknesses
- Error not dependent on slice thickness
- Error approximately 0.2%



#### Error Plots from 3 Time Points from Patients

Data courtesy of V. Stevenson, D. Miller et al., ION, London

- 39 patients (white-matter atrophy)
- Three time points
- Test accuracy by to->t2 vs to->t1 + t1->t2
- Errors within 0.2%



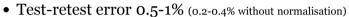
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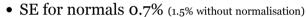
## SIENAX: Cross-Sectional Atrophy

- BET: find brain and skull
- FLIRT: use brain & skull to normalise to standard space
- Use standard space mask to cut brain stem and ensure no optic nerve/eyeballs
- Tissue segmentation (FAST, including partial volume estimation)
- Gives (normalised) brain (and grey & white) volume

#### Cross-Sectional Atrophy: Brain State

- Example: SIENAX (from FSL)
- Measures brain volume normalised for head size
- Proven for T1, T2, PD etc.

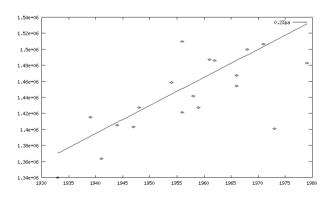






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## Normalised Brain Volume vs DoB (Normals)



#### SIENAX Results: MS vs Controls

Group	N	Mean Volume /10 <sup>6</sup> mm <sup>3</sup>	SD /10 <sup>6</sup> mm <sup>3</sup>	P
Controls	20	1.45	0.05	
Total MS	72	1.39	0.10	0.0001
EDSS <2	33	1.44	0.07	
EDSS <5	61	1.41	0.09	0.01
EDSS 2-4	27	1.38	0.10	0.0001
EDSS 5-8	10	1.27	0.10	0.0001

- Data from Siena, Italy
- ANOVA Tukey shows significant difference between controls and all EDSS bins except for EDSS<2</li>

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## Voxelwise Cross-Subject Statistics - SIENAr

Extend SIENA for voxelwise cross-subject statistics, e.g.:

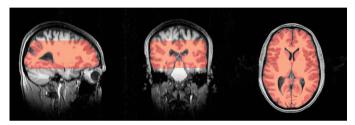
- where is atrophy different between two groups,
- or where does atrophy correlate with EDSS
- run SIENA to get edge "flow" image
- dilate
- transform to standard space
- mask with standard-space edge-mask
- blur (optional)
- carry out voxelwise cross-subject statistics



#### Cross-Subject Comparisons (Partial Head Images)

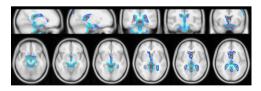
If different subjects have varying amounts of head in field of view, atrophy comparisons are not valid. Therefore use standard-space-based masking or Z limits so that all is consistent.

For example, to only use data where -20mm < Z < +50mm (in standard space), use options -b -20 -t 50



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## Voxelwise Cross-Subject Statistics - SIENAr

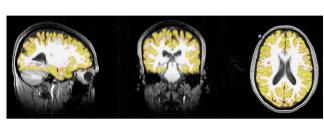


Example - one-group MS atrophy

## Regional Atrophy Measurement - SIENAX

#### With SIENAX, carry out regional breakdown

This gives peripheral GM volume and ventricular CSF volume, using standard-space masks.





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#### References

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#### Voxelwise Volumetry - VBM

- VBM: Voxelwise structural stats, e.g. with SPM or SIENAX+IRTK(nonlinear reg):
- Segment -> GM PVE
- Align to standard space (with density modulation)
- Voxelwise cross-subject stats
- Pros: fully automated, easy to test whole brain
- Con: ambiguity between cross-subject geometry shifts and intensity changes...hard to interpret results sometimes

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